ELEC ENG 3BB3: Cellular Bioelectricity

Notes for Lecture 17 Tuesday, February 11, 2014

Linear (subthreshold) response of a cylindrical fiber:

Under subthreshold conditions, the transmembrane current per unit length i_m (mA/cm) in a cylindrical fiber is:

$$i_m = \frac{v_m}{r_m} + c_m \frac{\mathrm{d}v_m}{\mathrm{d}t},\tag{7.12}$$

where r_m is the membrane resistance times unit length (Ωcm) and c_m is the membrane capacitance per unit length ($\mu F/cm$). Dependence of i_m on V_m (cont.): If Eqns. (6.8) is differentiated with respect to x, then:

$$\frac{\partial^2 V_m}{\partial x^2} = -(r_i + r_e) \frac{\partial I_i}{\partial x} + r_e \frac{\partial I}{\partial x}.$$
 (6.10)

Substituting Eqns. (6.3) and (6.6) gives:

$$\frac{\partial^2 V_m}{\partial x^2} = (r_i + r_e) i_m + r_e i_p \qquad (6.11)$$
$$\Rightarrow i_m = \frac{1}{(r_i + r_e)} \left(\frac{\partial^2 V_m}{\partial x^2} - r_e i_p \right). \quad (6.12)$$

Linear (subthreshold) response of a cylindrical fiber (cont.):

Substituting Eqn. (7.12) into cable equation (6.11) gives:

$$\lambda^2 \frac{\partial^2 v_m}{\partial x^2} - \tau \frac{\partial v_m}{\partial t} - v_m = r_e \lambda^2 i_p, \quad (7.14)$$

where:

$$\lambda = \sqrt{\frac{r_m}{r_i + r_e}}$$
 and $\tau = r_m c_m$. (7.15)

Steady-state solution for stimulus current at the origin:

Injection of a small current into the extracellular space at the origin (center) of an infinitely-long cylindrical fiber can be approximated by a spatial delta function source:

$$i_p = I_0 \,\delta(x) \,,$$
 (7.22)

where I_0 is the total applied current (mA) and $\delta(x)$ is the unit delta function.

Note that i_p is zero everywhere except at the origin, where it is infinite, and integrating i_p around the origin gives the total current I_0 .

Steady-state solution for stimulus current at the origin (cont.):

Solving Eqn. (7.14) under these conditions gives:

$$v_m = -\frac{r_e \lambda I_0}{2} e^{-|x|/\lambda}$$
. (7.34)

In Eqn. (7.34), the constant λ describes the rate of decay of the steady-state membrane potential as a function of *distance* along the cylindrical fiber.

Thus, it is referred to as the **space constant**.

Space constant properties:

For a cylindrical fiber with uniform membrane properties and with $r_e \frac{1}{4} 0$:

$$\lambda = \sqrt{\frac{r_m}{r_i + r_e}} \approx \sqrt{\frac{r_m}{r_i}}.$$
 (7.19)

Substituting for r_i and r_m in Eqn. (7.19) using Eqns. (2.55[°]) and (2.56[°]) gives:

$$\lambda = \sqrt{\frac{R_m/2\pi a}{R_i/\pi a^2}}$$
(7.20)
$$= \sqrt{\frac{aR_m}{2R_i}}.$$
(7.21)

Normalized space and time notation:

To simplify our notation, we introduce the normalized space and time variables:

$$X = \frac{x}{\lambda}$$
 and $T = \frac{t}{\tau}$, (7.36)

such that the homogenous version of Eqn. (7. 14) becomes:

$$\frac{\partial^2 v_m}{\partial X^2} - \frac{\partial v_m}{\partial T} - v_m = 0.$$
 (7.37)

If we assume an unbounded extracellular space and an intracellular injected step current, we can assume that $r_e \frac{1}{4} 0$.

In the normalized space and time variables the time-varying solution is:

$$v_m(X,T) = \frac{r_i \lambda I_0}{4} \left\{ e^{-|X|} \left[1 - erf\left(\frac{|X|}{2\sqrt{T}} - \sqrt{T}\right) \right] - e^{|X|} \left[1 - erf\left(\frac{|X|}{2\sqrt{T}} + \sqrt{T}\right) \right] \right\}, \quad (7.48)$$

Converting back to the original coordinates gives:

$$v_m(x,t) = \frac{r_i \lambda I_0}{4} \left\{ e^{-|x|/\lambda} \left[1 - \operatorname{erf}\left(\frac{|x|}{2\lambda}\sqrt{\frac{\tau}{t}} - \sqrt{\frac{t}{\tau}}\right) \right] - e^{|x|/\lambda} \left[1 - \operatorname{erf}\left(\frac{|x|}{2\lambda}\sqrt{\frac{\tau}{t}} + \sqrt{\frac{t}{\tau}}\right) \right] \right\}$$
(7.49)

where:

$$\operatorname{erf}(y) \stackrel{\Delta}{=} \frac{2}{\sqrt{\pi}} \int_0^y \mathrm{e}^{-z^2} \mathrm{d}z.$$
 (7.50)

For a given value of time, the spatial behaviour is exponential-like. For $t > \tau$, $v_m(x)$ tends towards a true exponential, as was obtained for the steady-state response described by Eqn. (7.34).

This continuous decrement of $v_m(x)$ with increasing jxj is due to the leakage of current through the membrane, while λ describes the rate of this effect.

For a given position x along a fiber, the membrane potential reaches its steady-state in an exponential-like manner over time.

Only at $x = \lambda$ is it truly exponential, i.e., the fraction of the steady-state potential that is achieved at $t = \tau$ is 1; 1/e.

Table 7.2. Temporal Morphology at Different Values of x Due to Current Step at x = 0

x	Fraction of steady-state value reached at $t = \tau$
0	0.843
λ	0.632
2λ	0.372
3λ	0.157
4λ	0.0453
5λ	0.00862



Figure 7.4. Theoretical distribution of potential difference across a passive nerve membrane in response to onset (*a* and *c*) and cessation (*b* and *d*) of a constant current applied intracellularly at the point x = 0. (a) and (b) show the spatial distribution of potential difference at different times, and (*c*) and (*d*) show the time course of the potential at different distances along the axon. Time (*t*) is expressed in units equal to the time constant, τ , and distance (*x*) is expressed in units of space constant, λ . [From D. J. Aidley, *The Physiology of Excitable Cells*, Cambridge University Press, Cambridge, 1978. After A. L. Hodgkin and W. A. H. Rushton, The electrical constants of a crustacean nerve fiber, *Proc. R. Soc. London, Ser. B* 133:444–479 (1946). Reprinted with permission of Cambridge University Press.]

Consider the source-fiber geometry shown to the right.



Figure 7.5. Geometry of source and fiber. A single current point source of magnitude I_0 is placed at a distance h from a circular cylindrical fiber of length 2L. The extracellular region is unbounded, uniform, and has a conductivity σ_e . The fiber radius is a and its intracellular conductivity is σ_i . The fiber's centerline lies along the coordinate z axis. The length is divided into elements Δz for numerical calculations.

The resulting extracellular field is:

$$\phi_a = \frac{I_0}{4\pi\sigma_e r},\tag{7.55}$$

where I₀ is the current strength, σ_{e} is the conductivity of the extracellular medium, and r is the distance from the source to an arbitrary field point.

Note that the effect of the fiber on the field is typically ignored.

Reformulating Eqn. (6.13) gives:

$$r_i i_m = \frac{\partial^2 \phi_i}{\partial z^2}, \qquad (7.56)$$

where z now defines the axial (longitudinal) coordinate.

The transmembrane current i_m must also equal the intrinsic ionic plus capacitive current of the membrane.

Replacing ϕ_i by $v_m + \phi_e$ and i_m by $i_{ion} + c_m \partial v_m / \partial t$ in Eqn. (7.56) gives:

$$r_i \frac{\partial v_m}{\partial t} = \frac{1}{c_m} \left(-i_{\text{ion}} r_i + \frac{\partial^2 v_m}{\partial z^2} + \frac{\partial^2 \phi_e}{\partial z^2} \right). \quad (7.57)$$

At rest, $v_m = 0$ for all z) $\partial^2 v_m / \partial z^2 = 0$ and $i_{ion} = v_m / r_m = 0$. Consequently, when the stimulus is first applied:

$$r_i \frac{\partial v_m}{\partial t} = \frac{1}{c_m} \frac{\partial^2 \phi_e}{\partial z^2}.$$
 (7.59)

Thus, the region where excitation is possible is where $\partial^2 \phi_e / \partial z^2$ is positive, because this will make $\partial v_m / \partial t$ initially positive.

Conversely, regions where $\partial^2 \phi_e / \partial z^2$ is negative will hyperpolarize, because this will make $\partial v_m / \partial t$ initially negative.

Consequently, the function $\partial^2 \phi_e / \partial z^2$ has been named the *activating function*.



Figure 7.6. Time evolution of the induced transmembrane voltage along a fiber. Stimulus duration is shown in milliseconds. The point current stimulus is at distance h = 0.02 cm from a fiber described in Fig. 7.5. Other parameters are $\lambda = 0.086$ cm, $\tau = 1.5$ msec, $\sigma_e = 33.3$ mS/cm, and $I_0 = -0.44$ mA. Note the region which is initially hyperpolarized but becomes depolarized. The activating function is similar to the 0.01-msec curve. [From R. Plonsey and R. C. Barr, Electric field stimulation of excitable tissue, *IEEE Trans. Biomed. Eng.* **42**:329–336 (1995). Copyright 1995, IEEE.]



Figure 7.7. Threshold values of v_m versus stimulus duration. Inset: Patch geometry. The transmembrane voltage at the end of the stimulus is shown for a stimulus condition that is just below threshold. Patch data are for the condition of no spatial variation. All potentials shown are relative to a baseline of $^{-57}$ mV. Outer: Each curve is for a different source-fiber distance as shown (*h* given in cm). Results shown are for z = 0, the shortest fiber-stimulus distance. Membrane properties are: $E_K = -72.1$ mV, $E_{\text{Na}} = 52.4 \text{ mV}, \overline{g}_{\text{Na}} = 120 \text{ mS/cm}^2, \overline{g}_K = 36 \text{ mS/cm}^2, g_I = 0.30 \text{ mS/cm}^2$. Fiber properties are: $R_m = 0.148 \text{ }\Omega \text{ cm}^2, \lambda = 0.086 \text{ cm}, C_m = 1.0 \text{ }\mu\text{F/cm}^2$. [From R. C. Barr and R. Plonsey, Threshold variability in fibers with field stimulation of excitable membranes. *IEEE Trans. Biomed. Eng.* 42:1185-1191 (1995). Copyright 1995, IEEE.]



Figure 7.8. Transmembrane potential as a function of time for stimuli which are just below and just above threshold. **Inset**: Curve A is for a just transthreshold stimulus and B for a just subthreshold stimulus. The source-fiber distance is 0.01 cm. Stimulus magnitudes were 1.40 mA (A) and 1.30 mA (B). **Outer**: Temporal responses for just subthreshold stimuli for stimulus duration as shown (in msec). [From R. C. Barr and R. Plonsey, Threshold variability in fibers with field stimulation of excitable membranes, *IEEE Trans. Biomed. Eng.* **42**:1185–1191 (1995) Copyright 1995 IEEE.]



Figure 7.9. Spatial distribution of transmembrane potential, $v_m(z)$, at the end of the stimulus. Each curve is labeled with the duration of the stimulus. The source-fiber distance is 0.10 cm. In each case the stimulus magnitude is for a just subthreshold response. [From R. C. Barr and R. Plonsey, Threshold variability in fibers with field stimulation of excitable membranes. *IEEE Trans. Biomed. Eng.* 42:1185-1191 (1995). Copyright 1995 IEEE.]