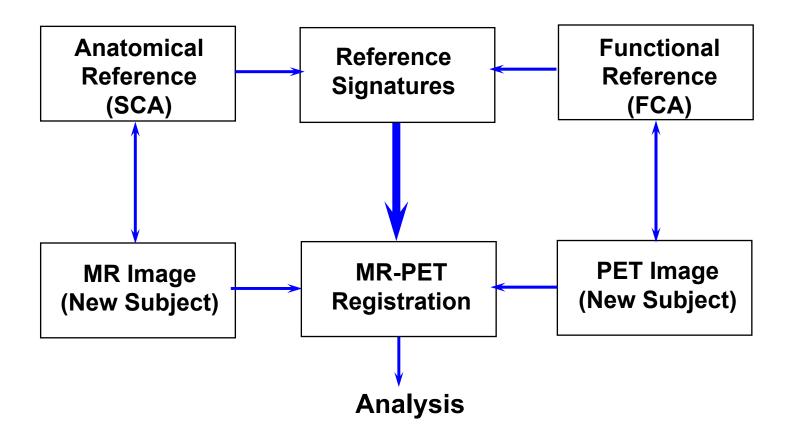
# ENG4BF3 Medical Image Processing

Image Registration



## What is image registration?

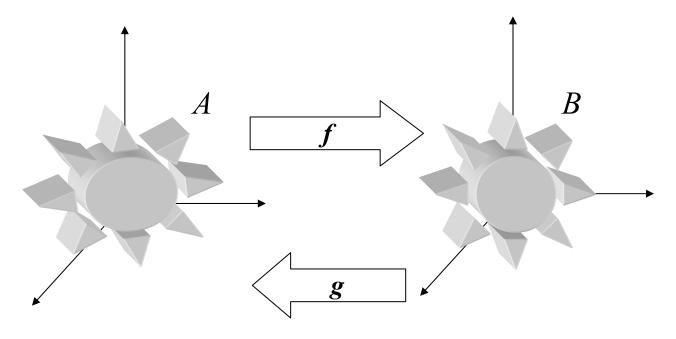
- Image Registration is the process of estimating an optimal transformation between two images.
- Sometimes also known as "Spatial Normalization".
- Applications in medical imaging
  - Matching PET (metabolic) to MR (anatomical) Images
  - Atlas-based segmentation/brain stripping
  - fMRI Specific
    - ➤ Motion Correction
    - ➤ Correcting for Geometric Distortion in EPI
    - ➤ Alignment of images obtained at different times or with different imaging parameters
      - Formation of Composite Functional Maps



A schematic diagram of multi-modality MR-PET image analysis using computerized atlases.



## Image Registration Through Transform

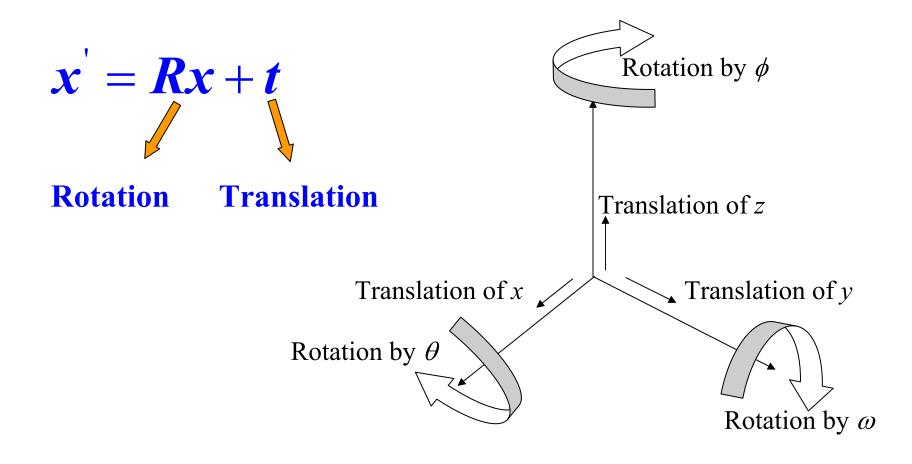


- Image registration provides transformation of a source image space to the target image space.
- The target image may be of different modalities from the source one.

## Multi-modality brain image registration

- External Markers and Stereotactic Frames Based Landmark Registration.
- Rigid-Body Transformation Based Global Registration.
- Image Feature Based Registration.
  - Boundary and Surface Matching Based Registration
  - Image Landmarks and Features Based Registration







$$x' = x + p$$

$$y' = y$$

$$z' = z$$

(a) Translation along x-axis by p (c) Translation along z-axis by r

$$x' = x$$

$$y' = y$$

$$z' = z + r$$

(b) Translation along y-axis by q

$$x' = x$$

$$y' = y + q$$

$$z' = z$$



(a) Rotation about x-axis by  $\theta$ 

$$x' = x + p$$

$$y' = y \cos \theta + z \sin \theta$$

$$z' = -y \sin \theta + z \cos \theta$$

(b) Rotation about y-axis by ω

$$x' = x \cos \omega - z \sin \omega$$
  
 $y' = y$   
 $z' = x \sin \omega + z \cos \omega$ 



(c) Rotation about z-axis by φ

$$x' = x \cos \varphi + y \sin \varphi$$

$$y' = -x \sin \varphi + y \cos \varphi$$

$$z' = z$$

$$x' = Rx + t$$

$$R = R_{\theta}R_{\omega}R_{\varphi} =$$

$$\begin{bmatrix} \cos \theta & \sin \theta & 0 \\ -\sin \theta & \cos \theta & 0 \\ 0 & 1 \end{bmatrix} \begin{bmatrix} \cos \omega & 0 & -\sin \omega \\ 0 & 1 & 0 \\ \sin \omega & 0 & \cos \omega \end{bmatrix} \begin{bmatrix} 1 & 0 & 0 \\ 0 & \cos \varphi & \sin \varphi \\ 0 & -\sin \varphi & \cos \varphi \end{bmatrix}$$

$$t = \begin{bmatrix} p \\ q \\ r \end{bmatrix}$$



$$x' = Rx + t$$

$$\begin{bmatrix} \mathbf{x}' \\ 1 \end{bmatrix} = \begin{bmatrix} \mathbf{R} & \mathbf{t} \\ \mathbf{0} & 1 \end{bmatrix} \begin{bmatrix} \mathbf{x} \\ 1 \end{bmatrix}$$



#### Rigid-Body Transformation: Affine Transform

**Affine transform: translation + rotation + scaling** 

Scaling: 
$$x' = ax$$

$$y' = by$$

$$z' = cz$$

a, b and c are scaling parameters in the three directions.

Affine transform can be expressed as

$$\begin{bmatrix} \mathbf{x}' \\ 1 \end{bmatrix} = \mathbf{A} \begin{bmatrix} \mathbf{x} \\ 1 \end{bmatrix}$$



#### Rigid-Body Transformation: Affine Transform

$$\begin{bmatrix} \mathbf{x}' \\ 1 \end{bmatrix} = \mathbf{A} \begin{bmatrix} \mathbf{x} \\ 1 \end{bmatrix}$$

A: The affine transform matrix that integrates translation, rotation and scaling effects.

$$\boldsymbol{A} = \begin{bmatrix} \boldsymbol{R} & \boldsymbol{t} \\ \boldsymbol{0} & 1 \end{bmatrix} \begin{bmatrix} \boldsymbol{S} & 0 \\ \boldsymbol{0} & 1 \end{bmatrix} \quad \text{where} \quad \boldsymbol{S} = \begin{bmatrix} \boldsymbol{a} \\ \boldsymbol{b} \\ \boldsymbol{c} \end{bmatrix}$$



#### Rigid-Body Transformation: Affine Transform

#### The overall mapping can be expressed as

$$\begin{bmatrix} x' \\ y' \\ z' \\ 1 \end{bmatrix} = \begin{bmatrix} 1 & 0 & 0 & p \\ 0 & 1 & 0 & q \\ 0 & 0 & 1 & r \\ 0 & 0 & 0 & 1 \end{bmatrix} \begin{bmatrix} \cos \theta & \sin \theta & 0 & 0 \\ -\sin \theta & \cos \theta & 0 & 0 \\ 0 & 0 & 1 & 0 \\ 0 & 0 & 0 & 1 \end{bmatrix} \begin{bmatrix} \cos \omega & 0 & -\sin \omega & 0 \\ 0 & 1 & 0 & 0 \\ \sin \omega & 0 & \cos \omega & 0 \\ 0 & 0 & 0 & 1 \end{bmatrix}$$

$$\begin{bmatrix} 1 & 0 & 0 & 0 \\ 0 & \cos \varphi & \sin \varphi & 0 \\ 0 & -\sin \varphi & \cos \varphi & 0 \\ 0 & 0 & 1 \end{bmatrix} \begin{bmatrix} a & 0 & 0 & 0 \\ 0 & b & 0 & 0 \\ 0 & 0 & c & 0 \\ 0 & 0 & 0 & 1 \end{bmatrix} \begin{bmatrix} x \\ y \\ z \\ 1 \end{bmatrix}$$



Principal axes registration (PAR) is used for global matching of binary volumes from CT, MR or PET images.

$$B(x, y, z) = \begin{cases} 1 & (x, y, z) \in object \\ 0 & (x, y, z) \notin object \end{cases}$$

$$(x_g, y_g, z_g)^T \longrightarrow \text{centroid of } B(x, y, z)$$

$$x_{g} = \frac{\sum_{x,y,z} xB(x,y,z)}{\sum_{x,y,z} B(x,y,z)} y_{g} = \frac{\sum_{x,y,z} yB(x,y,z)}{\sum_{x,y,z} B(x,y,z)} z_{g} = \frac{\sum_{x,y,z} zB(x,y,z)}{\sum_{x,y,z} B(x,y,z)}$$



The principal axes of B(x,y,z) are the eigenvector of inertia matrix I:

$$I = \begin{bmatrix} I_{xx} & -I_{xy} & -I_{xz} \\ -I_{yx} & I_{yy} & -I_{yz} \\ -I_{zx} & -I_{zy} & I_{zz} \end{bmatrix}$$

$$I_{xx} = \sum_{x,y,z} \left[ (y - y_g)^2 + (z - z_g)^2 \right] B(x,y,z)$$

$$I_{yy} = \sum_{x,y,z} \left[ (x - x_g)^2 + (z - z_g)^2 \right] B(x,y,z)$$

$$I_{zz} = \sum_{x,y,z} \left[ (x - x_g)^2 + (y - y_g)^2 \right] B(x,y,z)$$

$$I_{xy} = I_{yx} = \sum_{x,y,z} \left[ (x - x_g)(y - y_g) \right] B(x,y,z)$$

$$I_{xz} = I_{zx} = \sum_{x,y,z} \left[ (x - x_g)(z - z_g) \right] B(x,y,z)$$

$$I_{yz} = I_{zy} = \sum_{x,y,z} \left[ (y - y_g)(z - z_g) \right] B(x,y,z)$$
CMaster

- $\Box$  The inertia matrix I is diagonal when computed with respect to the principal axes.
- ☐ The centroid and principal axes can describe the orientation of a volume.
- ☐ The principal axes registration can resolve six degrees of freedom of an object (three rotation and three translation).
- ☐ It can compare the orientations of two binary volumes through rotation, translation and scaling.



Normalize the principal axes (the eigenvectors of *I*) and define:

$$E = \begin{bmatrix} e_{11} & e_{12} & e_{13} \\ e_{21} & e_{22} & e_{23} \\ e_{31} & e_{32} & e_{33} \end{bmatrix}$$

The rotation matrix is

$$\begin{aligned} & \boldsymbol{R} = R_{\theta} R_{\omega} R_{\varphi} = \\ & \begin{bmatrix} \cos \theta & \sin \theta & 0 \\ -\sin \theta & \cos \theta & 0 \\ 0 & 0 & 1 \end{bmatrix} \begin{bmatrix} \cos \omega & 0 & -\sin \omega \\ 0 & 1 & 0 \\ \sin \omega & 0 & \cos \omega \end{bmatrix} \begin{bmatrix} 1 & 0 & 0 \\ 0 & \cos \varphi & \sin \varphi \\ 0 & -\sin \varphi & \cos \varphi \end{bmatrix} \end{aligned}$$



Let

$$E = R$$

We can resolve the rotation angles as

$$\omega = \arcsin(e_{31})$$

$$\theta = \arcsin(-e_{21}/\cos\omega)$$

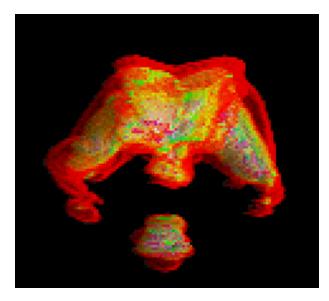
$$\varphi = \arcsin(-e_{32}/\cos\omega)$$



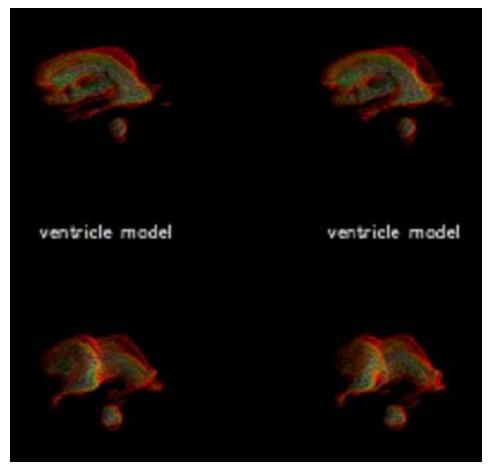
#### The PAR algorithm to register V1 and V2:

- ▶1. Compute the centroid of V1 and translate it to the origin.
- $\triangleright$ 2. Compute the principal axes (by using E=R) of V1 and rotate V1 to coincide with the x, y and z axes.
- ➤3. Compute the principal axes of V2 and rotate the x, y and z axes to coincide with it.
- ▶4. Translate the origin to the centroid of V2.
- >5. Scaling V2 to match V1 by using factor  $F_s = \sqrt[3]{V1/V2}$ .





A 3-D model of brain ventricles obtained from registering 22 MR brain images using the PAR method.



Rotated views of the 3-D brain ventricle model in the left image.



## Iterative Principal Axes Registration (IPAR)

Advantages over PAR: IPAR can be used with partial volumes.

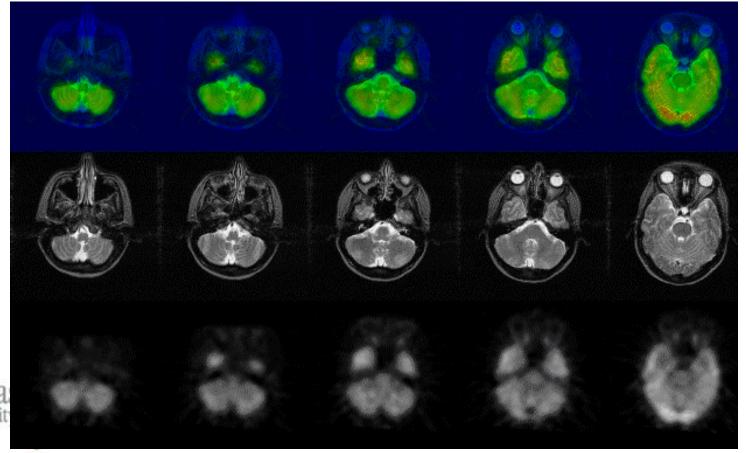
Assumption made in IPAR: the field of view (FOV) of a functional image (such as PET)) is less than the full brain volume while the other volume (such as MR image) covers the entire brain.

Algorithm: refer to pages 259 ~ 264 of the textbook.



# Iterative Principal Axes Registration (IPAR)

Sequential slices of MR (middle rows) and PET (bottom rows) and the registered MR-PET brain images (top row) using the IPAR method.



## Landmarks and Features Based Registration

- ➤ With the corresponding landmarks/features identified in the source and target images, a transformation can be computed to register the images.
- Non-rigid transformations have been used in landmarks/features based registration by exploiting the relationship of corresponding points/features in source and target images.
- > Two point-based algorithms will be introduced.



## Similarity Transformation

X: source image

Y: target image

x: landmark points in X

y: landmark points in Y

T(x): non-rigid transformation

$$x' = T(x) = s \cdot r \cdot x + t$$

scaling rotation translation



## Similarity Transformation

The registration error:

$$E(x) = T(x) - y = srx + t - y$$

The optimal transform is to find s, r and t to minimize:

$$\sum_{i=1}^{N} w_i^2 \left| srx_i + t - y_i \right|^2$$

 $w_i$ : the weighting factor for landmark  $x_i$ 

N: the number of landmark points



## Similarity Transformation: Algorithm

- 1. Set s=1.
- 2. Find *r* through the following steps:
  - 2a) Compute the weighted centroids of x and y.

$$\overline{\boldsymbol{x}} = \frac{\sum_{i=1}^{N} w_i^2 \boldsymbol{x}_i}{\sum_{i=1}^{N} w_i^2} \qquad \overline{\boldsymbol{y}} = \frac{\sum_{i=1}^{N} w_i^2 \boldsymbol{y}_i}{\sum_{i=1}^{N} w_i^2}$$

*2b)* Compute the distance of each landmark from the centroid.



$$\overline{\boldsymbol{x}}_i = \boldsymbol{x}_i - \overline{\boldsymbol{x}} \qquad \overline{\boldsymbol{y}}_i = \boldsymbol{y}_i - \overline{\boldsymbol{y}}$$

# Similarity Transformation: Algorithm (continued)

2c) Compute the weighted co-variance matrix.

$$\mathbf{Z} = \sum_{i=1}^{N} w_i^2 \overline{\mathbf{x}}_i \overline{\mathbf{y}}_i^t$$

Singular value decomposition

$$Z = U \Lambda V^{t}$$

where

$$UU^t = VV^t = I$$

$$\Lambda = diag(\lambda_1, \lambda_2, \lambda_3) \quad \lambda_1 \ge \lambda_2 \ge \lambda_3 \ge 0$$

#### 2d) Compute



$$r = V \cdot diag(1, 1, \det(VU)) \cdot U^{t}$$

# Similarity Transformation: Algorithm (continued)

3. Compute the scaling factor:

$$S = \frac{\sum_{i=1}^{N} w_i^2 r \overline{x}_i \overline{y}_i}{\sum_{i=1}^{N} w_i^2 r \overline{x}_i \overline{x}_i}$$

4. Compute

$$t = \overline{y} - sr\overline{x}$$



## Iterative Features Based Registration (WFBR)

 $X_i$ : a data set representing a shape in source image

 $Y_i$ : the corresponding data set in target image

 $x_{ij}$ : points in  $X_i$   $y_{ij}$ : points in  $Y_i$ 

T(x): transform operator

$$\mathbf{x}' = T(\mathbf{x}) = s \cdot \mathbf{r} \cdot \mathbf{x} + \mathbf{t}$$

**Disparity function to be minimized:** 

$$d(T) = \sqrt{\sum_{i=1}^{N_s} \sum_{j=1}^{N_i} w_{ij}^2 \| T(\mathbf{x}_{ij}) - \mathbf{y}_{ij} \|^2}$$

 $N_s$ : number of shapes

 $N_i$ : number of points in shape  $X_i$ 

## WFBR: Iterative Algorithm

- 1. Determine *T* by the similarity transformation method.
- 2. Let  $T^{(0)}=T$  and initialize the optimization loop for k=1 as

$$\mathbf{x}_{ij}^{(0)} = \mathbf{x}_{ij}$$
$$\mathbf{x}_{ij}^{(1)} = T^{(0)}(\mathbf{x}_{ij}^{(0)})$$

3. For the points in shape  $X_i$ , find the closest points in  $Y_i$  as

$$\mathbf{y}_{ij}^{(k)} = C_i(\mathbf{x}_{ij}^{(k)}, Y_i) \quad j = 1, 2, 3, ..., N_i$$

where  $C_i$  is the operator to find the closest point.



## WFBR: Iterative Algorithm (continued)

4.Compute the transformation  $T^{(k)}$  between  $\{x_{ij}^{(0)}\}$  and  $\{y_{ij}^{(k)}\}$  with the weights  $\{w_{ij}\}$  using the similarity transformation method.

#### 5. Compute

$$\mathbf{x}_{ij}^{(k+1)} = T^{(k)}(\mathbf{x}_{ij}^{(0)})$$

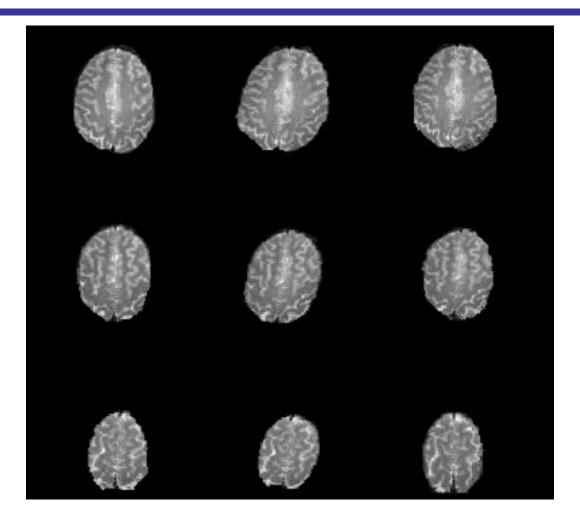
6. Compute  $d(T^{(k)}) - d(T^{(k+1)})$ . If the convergence criterion is met, stop; otherwise go to step 3 for the next iteration.



## Elastic Deformation Based Registration

- One of the two volume is considered to be made of elastic material while the other serves as a rigid reference. Elastic matching is to map the elastic volume to the reference volume.
- ☐ The matching starts in a coarse mode followed by fine adjustments.
- ☐ The constraints in the optimization include smoothness and incompressibility.
- ☐ The smoothness ensures that there is continuity in the deformed volume while the incompressibility guarantee that there is no change in the total volume.
- $\square$  For detail algorithm, refer to pp. 269 ~ 272 in the textbook.





Results of the elastic deformation based registration of 3-D MR brain images: The left column shows three reference images, the middle column shows the images to be registered and the right column shows the registered brain images.

### **End of Lecture**

